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54 External ear canal electrode to be placed proximate the tympanic membrane and method of stimulating/recording
 utilizing external ear canal electrode placed proximate the tympanic membrane.

57 An electrode (10) adapted to be utilized within the external ear canal (46) for applying/recording electrical signals to/from the neural/neuromuscular system of a person having an external ear canal (46) and adjacent tympanic membrane (48). The electrode (10) utilizes an elongated flexible body (12) having a proximate end (14) and a distal end (16). A compressible material (18) is mounted at the distal end (16) of the body (12) and an electrically conductive gel (20) is carried by the compressible material (18). An electrical conductor (22) communicates with the body (12) and electrically couples the conductive gel (20) to the proximate end (14) of the electrode (10). A method (30) of stimulating the neural/neuromuscular system of a person comprising the steps of inserting (32) an electrode (10) of this design into the external ear canal (46) with the electrode (10) being positioned with the electrically conductive gel (20) proximate the tympanic membrane (48) or tympano-meatal annulus (50). A second return electrode is applied (34) to the body and an electrical stimulus signal is applied (36) to the electrode pair. A method (38) of recording electrical signals from the neural/neuromuscular system of a person having a body and an external ear canal (46) and adjacent tympanic membrane (48) utilizes the steps of inserting (40) an electrode (10) of this design into the external ear canal (46) of the person with the electrode (10) being positioned with the electrically conductive gel (20) proximate the tympanic membrane (48). A second reference electrode is applied

(42) to the body of the person and electrical signals are then recorded (44) from the electrode pair.

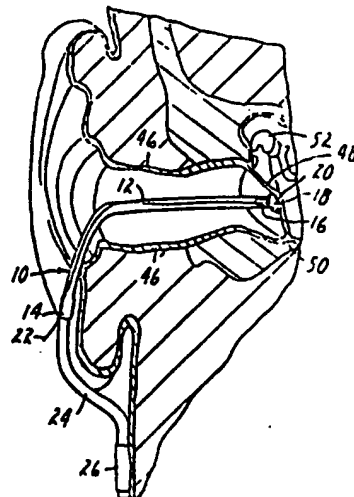


FIG. 4

AN EXTERNAL EAR CANAL ELECTRODE TO BE
PLACED PROXIMATE THE TYMPANIC MEMBRANE AND
METHOD OF STIMULATING/RECORDING UTILIZING EXTERNAL
EAR CANAL ELECTRODE PLACED PROXIMATE THE
TYMPANIC MEMBRANE

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Technical Field

The present invention relates generally to electrodes for and methods of applying/recording electrical signals to/from the neural/neuromuscular system of a person. The present invention more particularly relates to such electrodes which are inserted into the external ear canal of a person and methods therefor.

Background Art

It is well known that electrical stimulation of the auditory system of a person can produce complex perceptions of sounds in human subjects. Experiments by Volta occurred in the early 1800's. Volta inserted metal bars into his external ear canals and passed current between the bars and reported the perception of sound. A series of studies was performed in the late 1930's by Jones, Stevens and Lurie which examined the relationship between various parameters of electrical stimulation and the listed auditory percepts. In these experiments, investigators used metal electrodes placed into saline filled external ear canals to deliver electrical current to the auditory system.

More recently, electrodes surgically implanted into the cochlea, are providing a sensation of hearing in profoundly deaf individuals. The development of cochlear implants has prompted significant additional research in the area of electrical stimulation for hearing augmentation.

Means of stimulating the auditory system which are noninvasive, as opposed to a cochlear implant, are desirable for several reasons. A noninvasive electrode system for auditory stimulation could be used as a functional auditory prosthesis, as a tool in the diagnostic evaluation of potential candidates for cochlear implants or to record the electrical signals generated by an auditory system stimulated by other means.

Several investigators have reported the use of electrodes combined with a saline filled ear canal (known as a Bremmer type electrode) to provide a noninvasive means of auditory stimulation. This approach to the stimulation of the auditory system has a major drawback. Current passed into the saline solution spreads rapidly in all directions through the tissues of the ear and head. The same electrical current which activates the auditory nerve can also stimulate cutaneous nerve fibers thereby producing uncomfortable and, possibly, painful sensations.

Existing systems of auditory stimulation have significant disadvantages. Cochlear implants require surgical invasion of the body. Thus, cochlear implants are not practical for evaluation or diagnostic purposes, which involve temporary stimulation or recording. On the other hand, conventional external ear canal stimulation has significant limitations in dynamic range. The electrical current used in external ear canal stimulation must be above an amount to exceed the hearing threshold but must be below an amount which would produce pain within the external ear canal or, possibly, uncomfortable loud sensations.

Disclosure of Invention

The present invention solves these problems

by eliminating surgical invasion while substantially increasing the dynamic range of the stimulation signals which can comfortably be utilized.

5 The only direct physical pathway from the
external ear canal to the inner ear (aside from the
skull itself) is the tympanic membrane and the ossicular
chain. This tissue connection constitutes the major
pathway for current flow between the inner ear and the
external ear canal and visa versa. Electrical signals
10 which are generated inside a normally functioning cochlea
travel through surrounding tissues and can be recorded
from outside of the cochlea. This technique is clinically
known as electrocochleography (ECoG). The amplitude
of ECoG signals is largest at the surface of the cochlea,
15 the measurement of which is an invasive technique. For
noninvasive measurements, the amplitude of ECoG signals
is greatest at the tympanic membrane. This supports
the hypothesis that the ossicles are the lowest resistance
pathway by which current travels between the cochlea
and the external ear canal. The present invention provides
20 an electrode and a method of stimulating or recording
which takes advantage of this low resistance connection
between the inner ear and the external ear canal. The
electrode can be used to either stimulate the inner
25 ear with electrical current or, conversely, to measure
the electrical activity originating within the inner
ear without an invasive technique.

 The present invention provides a method of
stimulating the neural/neuromuscular system of a person
30 having a body and an external ear canal and adjacent
tympanic membrane. A first electrode is inserted into
the external ear canal of the person. The first electrode
has an elongated flexible body having a proximate end
and a distal end. The first electrode has a compressible
35 material mounted at the distal end of the elongate flexible

body and has an electrically conductive gel carried
by the compressible material. The first electrode has
an electrical conductor communicating with the elongate
flexible body being electrically coupled to the electrically
conductive gel. The first electrode is positioned with
5 the electrically conductive gel proximate the tympanic
membrane or the tympano-meatal annulus of the person.
A second return electrode is then applied to the body
of the person. An electrical stimulus signal is applied
to the electrode pair thereby stimulating the
10 neural/neuromuscular system of the person without surgically
invasive techniques. Optionally, an anesthetic may be
applied to the area of the tympanic membrane or
tympano-meatal annulus of the person to further increase
the dynamic range of the electrical stimulating signal.
15 This anesthetic may be incorporated into the conductive
gel, may be iontophoretically delivered, or may be injected.

The present invention also provides a method
of recording electrical signals from the
neural/neuromuscular system of a person having a body
20 and an external ear canal and an adjacent tympanic membrane.
A first electrode is inserted into the external ear
canal of the person. The first electrode has an elongate
flexible body having a proximate and a distal end. The
first electrode has a compressible material mounted
25 at the distal end of the elongate flexible body and
has an electrically conductive gel carried by the
compressible material. The first electrode further has
an electrical conductor communicating with the elongate
flexible body being electrically coupled to the electrically
30 conductive gel. The first electrode is positioned with
the electrically conductive gel proximate the tympanic
membrane or tympano-meatal annulus of the person. A
second reference electrode is then applied to the body
of the person. Electrical signals generated by the cochlea

of the person are then recorded utilizing the inserted electrode pair.

5 The present invention also provides an electrode adapted to be utilized within the external ear canal for applying/recording electrical signals to/from the neural/neuromuscular system of a person having an external ear canal and adjacent tympanic membrane. The electrode has an elongated flexible body having a proximate end and a distal end. A compressible material is mounted
10 at the distal end of the elongate flexible body. An electrically conductive gel is carried by the compressible material and an electrical conductor communicates with the elongate flexible body electrically coupling the electrically conductive gel and adapted to be coupled
15 to a stimulator/recorder at the proximate end. An electrode constructed in this fashion may be placed in the external ear canal with a distal end being proximate the tympanic membrane or tympano-meatal annulus so electrical signals can be applied/recorded to/from the neural/neuromuscular
20 system.

In an alternative embodiment, the electrically conductive gel is absorbed into the compressible material which, in another alternative embodiment, may also be resilient. The elongated flexible body is stiff enough
25 to enable it to be inserted into the external ear canal but flexible enough to bend if the electrode is pushed against the tympanic membrane without rupturing the tympanic membrane. In another alternative embodiment, an anesthetic may be carried by the compressible material.
30 In other alternative embodiments, a physical fixation device is utilized for physically securing the electrode with respect to the external ear canal. In alternative embodiments, the physical fixation device may be an inflatable cuff, radial fins, a resilient collar or
35 a coiled spring. In an alternative embodiment, adhesive

tape adhesively couples the elongated flexible body to the body of the person which in another embodiment may be utilized as a return/reference electrode. In a still further alternative embodiment, the compressible material may be connected to the distal end of the flexible body by a coiled spring.

Brief Description of Drawings

The foregoing advantages, construction and operation of the present invention will become more readily apparent from the following description and accompanying drawings in which:

Figure 1 is an illustration of an electrode of a preferred embodiment of the present invention;

Figure 2 is a illustration of a method of the present invention;

Figure 3 is an illustration of an alternative method of the present invention;

Figure 4 is an illustration of an electrode of the present invention inserted in an external ear canal;

Figure 5 is an illustration of an alternative embodiment of an electrode of the present invention with an inflatable cuff;

Figure 6 is an illustration of an alternative embodiment of an electrode of the present invention with an inflatable ring;

Figure 7 is an illustration of an alternative embodiment of an electrode of the present invention with a collar;

Figure 8 is an illustration of an alternative embodiment of an electrode of the present invention with fins;

Figure 9 is an illustration of an alternative embodiment of an electrode of the present invention with a speculum and an anesthetic delivery tube; and

Figure 10 is an illustration of an alternative embodiment of an electrode of the present invention with a spring tip.

Detailed Description of the Preferred Embodiments

5 A preferred embodiment of the electrode 10
of the present invention is illustrated in Figure 1.
The electrode 10 is formed from a length of silicone
elastomer tubing 12 forming an elongated flexible body.
The silicone elastomer tubing 12 is of a sufficient
10 size and sufficient stiffness to allow the insertion
of the electrode 10 into the external ear canal but
is flexible enough so that the silicone elastomer tubing
12 will bend and not create damage to the tympanic membrane
should the electrode 10 be inserted in position proximate
15 to tympanic membrane or tympano-meatal annulus. An example
of tubing 12 which is suitable for this purpose is Dow
Corning Medical Grade HP SilasticTM tubing with an outside
diameter of 0.08 inches (2.03 millimeters) and an inside
diameter of 0.077 inches (1.96 millimeters). The tubing
20 12 has a proximate end 14 suitable to be grasped by
the insertion means, such as the health care technician's
fingers, and a distal end 16 to be placed into the external
ear canal. A compressible material 18 is mounted at
the distal end 16 of silicone elastomer tubing 12. In
25 a preferred embodiment, the compressible material is
a sponge material such as an open cell compressible
foam such as a polyester/polyether sponge and is formed
to fit snugly within the distal end 16 of silicone
elastomer tubing 12. In a preferred embodiment, the
30 compressible material 18 has an overall diameter larger
than the diameter of silicone elastomer tubing 12. In
a preferred embodiment, the dimensions of the compressible
material 18 are about 0.25 inch (6.4 millimeters) in

diameter and about 0.125 inch (3.2 millimeters) in compressible distance. It is preferred that the compressible material also be resilient. The compressible material 18 cushions the tympanic membrane or tympano-meatal annulus when the electrode 10 is inserted approximately at that position. The resiliency in compressible material 18 will allow the electrode 10 to be withdrawn and reinserted with similar insertion characteristics on subsequent insertions into the external ear canal. A conductive gel is carried by the compressible material at the distal end 16 of silicone elastomer tubing 12. A preferred conductive gel is Red DotTM No. 2248 Solid Conductive Electrode Gel available from Minnesota Mining and Manufacturing Company. An electrical conductor, namely a wire, 22 is inserted through silicone elastomer tubing 12 from the proximate end 14 to the distal end 16 communicating with the conductive gel 20 carried by compressible material 18. Electrical conductor 22 provides the mechanism for supplying the electrical stimulus signal to the distal end 16 of the electrode 10 or to conduct electrical signals generated by the cochlea from the conductive gel 20 to the proximate end 14 of the electrode 10. It is important to electrically insulate electrical conductor 22 from the walls of the external ear canal and is covered with insulation such as TeflonTM insulation. In the preferred embodiment, electrical conductor 22 is carried in the interior of silicone elastomer tubing 12. In other embodiments, it is envisioned that the electrical conductor could be positioned outside of silicone elastomer tubing 12, spirally wrapped or otherwise communicating with silicone elastomer tubing 12 to create a conductive path between the conductive gel 20 at the distal end 16 and the proximate end 14 of electrode 10. A preferred electrical conductor

22 is a 0.003 inch (0.08 millimeters) diameter wire of 90% platinum and 10% iridium with TeflonTM insulation.

Those features of Figure 1 heretofor described contain all the essential features of the electrode 10. In addition, the preferred electrode 10 illustrated in Figure 1 has a second length of silicone elastomer tubing 24 affixed to the proximate end 14 of silicone elastomer tubing 12. One means of securing the second piece of silicone elastomer tubing 24 to silicone elastomer tubing 12 is to make silicone elastomer tubing 24 of a larger diameter and of such a diameter so that a snug fit is developed when silicone elastomeric tubing 24 is placed over or inside of the proximate end 14 of silicone elastomer tubing 12. In a preferred embodiment, electrical conductor 22 may exit the electrode at this point. An alternative electrode 22 could be carried with silicone elastomer tubing 24 the entire length of the electrode or exit somewhere in between. The flexibility characteristics of silicone elastomer tubing 12 are essential for the proper placement of the electrode 10 within the external ear canal. In a preferred embodiment, silicone elastomer tubing 24 is stiffer than and is less flexible than silicone elastomer tubing 12. This silicone elastomer tubing 12 may carry an adhesive tape 26 which can be used to secure the electrode 10 to the external ear, cheek or face of the user providing some mechanical stability to the electrode 10 when it is in place. Any commonly utilized adhesive tape 26 may be utilized such as MicroporeTM or DuraporeTM tape available from Minnesota Mining and Manufacturing Company.

An electrode constructed as described in Figure 1 affords several advantages over existing technology. The tip, or distal end 16, of the electrode 10 is composed of a compressible material 18, e.g., a sponge, which is infiltrated with a conductive gel 20. The main body

of the electrode 10 is a soft silicone elastomer tubing 12 which allows the insertion of the electrode 10 into the external ear canal. The flexibility of the silicone elastomer tubing 12 combined with the compressible material 18 and conductive gel 20 allows the electrode 10 to be positioned proximate the tympanic membrane or tympano-meatal annulus with little or no discomfort. The contact area of the conductive gel 20 with the tympanic membrane or tympano-meatal annulus results in a low impedance connection for recording or stimulating. It has been found that recording with an electrode of this design results in signals which are significantly greater in magnitude than those obtained with a bare conductive ball electrode and provide a more faithful representation of the electrical signals generated by the cochlea. Recording of inner ear potentials is useful in the clinical diagnosis of ear disorders. Further, electrical stimulation of the inner ear via this electrode 10 could be applied for prosthetic, i.e., hearing augmentation, therapeutic, i.e., tinnitus suppression, treatment of hydrops or other inner ear disorders, or diagnostic, i.e., testing of cochlear implant candidates, purposes. The design of the electrode 10 of the present invention affords that current flow into the cochlea is maximized when current is applied directly to the tympanic membrane or tympano-meatal annulus. Less current is lost into the surrounding tissues resulting in (a) lower thresholds for auditory stimulation and (b) less stimulation of cutaneous pain fibers.

Several variations of the electrode 10 could be made without departing from the scope of the present invention. An anesthetic 28 could be incorporated in the compressible material 18. This anesthetic would provide local anesthesia to the stimulus site to further reduce any discomfort from the stimulation or placement

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of electrode 10 proximate the tympanic membrane or tympano-meatal annulus. A preferred anesthetic to be utilized is lidocaine. Further, it is contemplated that the size of the electrode tip at the distal end 16 could be varied depending upon the optimal use of the electrode, as for example, for stimulation or for recording. For stimulation purposes, a relatively large tip would be optimal since lower current densities at the point of contact would be obtained. A relatively smaller tip at the distal end 16 of the electrode 10 would be optimal for recording purposes where the tip of the electrode 10 would not load or impede the movement of the tympanic membrane.

To insert the electrode 10 into the external ear canal, an insertion tool, typically the health care technician's fingers, grasps the silicone elastomeric tubing 12 and inserts the distal end 16 into the ear canal. The electrode 10 which contains the conductive gel 20, resilient material 18 and, optionally, an anesthetic, if desired, is guided down the external ear canal until the conductive gel 20 of the electrode 10 contacts the tympanic membrane or tympano-meatal annulus. The electrode 10 may then be held in place or may be secured by appropriate physical fixation means, as for example, adhesive tape 26. Electrical conductor 22 may then be connected to the appropriate instrument for either stimulating the inner ear or recording of signals from the inner ear.

Figure 2 illustrates a method 30 of stimulating the neural/neuromuscular system of a person having a body and an external ear canal and an adjacent tympanic membrane. A first electrode is inserted 32 proximate the tympanic membrane or tympano-meatal annulus. In order to properly localize the current density characteristics and to restrain the electrical current

to the appropriate conductive path and to minimize
uncomfortableness or pain sensation within the external
ear canal, the first electrode should have an elongated
flexible body with a proximate end and a distal end.
5 A compressible material is mounted at the distal end
of the body. A conductive gel 20 is carried by the
compressible material and an electrical conductor
communicates with the elongated flexible body and is
electrically coupled to the electrically conductive
10 gel. A second electrode is then applied 34 to the body.
It is not necessary that the second electrode be of
any particular design or that it be applied at any
particular location on the body. In general, conventional
cutaneous electrodes are applied to the scalp of a person
15 or perhaps to the cheek. The second electrode is a return
electrode. An electrical stimulus signal is then applied
36 to the electrode pair consisting of the first electrode
inserted in the external ear canal proximate the tympanic
membrane or tympano-meatal annulus and the second electrode
20 applied elsewhere to the body.

Similarly, Figure 3 illustrates a method of
recording 38 electrical signals from the
neural/neuromuscular system of a person having a body
and an external ear canal and adjacent tympanic membrane.
25 A first electrode is inserted 40 into the external ear
canal proximate the tympanic membrane or tympano-meatal
annulus. A first electrode similar to the electrode
described with respect to step 32 of Figure 2 is
appropriate. As in step 34 of Figure 2, a second electrode
30 is then applied 42 to the body of a person to serve
as a reference electrode. Similarly, this electrode
needs to be of no special design and maybe a conventional
cutaneous electrode applied to the scalp, cheek or other
portion of the body. The electrical conductors from
35 the electrode pair consisting of the first electrode

and the second electrode are then connected to a recording apparatus and the electrical signals obtained from the inner ear are recorded 44.

5 Figure 4 shows the electrode 10 of the present invention inserted into the external ear canal 46 of a patient. In particular, the electrode 10 shown in Figure 1 is illustrated. Silicone elastomer tubing 12 is stiff enough to be guided into the external ear canal but flexible enough to bend once contact is made with
10 the tympanic membrane 48. Alternatively, the electrode 10 could contact the tympano-meatal annulus 50. The conductive gel 20 of the electrode 10 contacts the tympanic membrane 48 or the tympano-meatal annulus 50. Compressible material 18 is compressed by the contact and positioning
15 of the electrode 10 proximate the tympanic membrane 48. Silastic tubing 24 continues outside the external ear canal 46 and is secured to the cheek of the patient by adhesive tape 26. Electrical conductor 22 may then be connected to the appropriate stimulating or recording
20 source or facility.

It can thus be seen, in reference to Figure 4, that the electrode 10 of the present invention, provides a relatively localized source of stimulation and recording at the tympanic membrane 48 or tympano-meatal annulus
25 50. Thus, the electrode 10 may take advantage of the most direct current pathway via the ossicular chain 52 to or from the inner ear. The flexibility of the silicone elastomer tubing and the compressibility of the compressible material 18 contribute to the avoidance
30 of pain due to the proximity of the electrode 10 to the tympanic membrane 48 or tympano-meatal annulus 50. Also contributing to the avoidance of pain is the localization of the currents such that stimulations of cutaneous nerve endings in the external ear canal
35 46 are minimized.

Once the electrode 10 has been placed in the external ear canal 46, it is advantageous to be able to physically fix the electrode 10 with respect to the external ear canal 46. Such fixation will allow consistency of stimulating or recording position as well as prevent damage to the tympanic membrane 48 due to movement of the electrode 10. Several alternative mechanical fixation techniques are described below.

In one alternative embodiment of the electrode 10, the adhesive tape 26 may be made conductive in the form of a cutaneous electrode and the adhesive tape 26 may form the second electrode described in the method of stimulating and the method of recording at steps 34 and 42, respectively, in Figures 2 and 3, respectively.

Figure 5 illustrates an alternative embodiment of an electrode 10. Again, the electrode 10 is formed with an elongated flexible body of a silicone elastomer tubing 12. A compressible material 18 is carried at the distal end 16 of the electrode 10. The compressible material contains a conductive gel 20. An electrical conductor 22 electrically communicates between the end of the electrode 10. Physical fixation of this electrode 10 is achieved through an inflatable cuff 54. Inflatable cuff 54 is preferably a cylindrical balloon constructed from silicone elastomer, preferably 7 mils (0.18 millimeters) thick, fashioned in a manner similar to that of an endotracheal tube and is affixed to silicone elastomer tubing 12. The electrode 10 may be inserted into the external ear canal with the inflatable cuff 54 in a deflated or relatively deflated condition thus allowing insertion of the electrode. Once the electrode has been placed proximate the tympanic membrane or tympano-meatal annulus, the inflatable cuff 54 may be inflated through the insertion of air into its body with a syringe. If removal of the electrode 10 or thereafter desired, the inflatable cuff 54 could be deflated through

the reverse process.

Figure 6 illustrates an electrode 10 similarly constructed as the electrode 10 in Figure 5. The electrode 10 in Figure 6 contains as a mechanical fixation means
5 an inflatable ring 56. Inflatable ring 56 may be constructed out of silicone elastomer material. Operating similarly to the inflatable cuff 54 of the electrode 10 of Figure 5, inflatable ring 56 may be in a relatively deflated condition prior to the insertion of the electrode 10
10 into the external ear canal. Again, once the electrode 10 is inserted into the external ear canal, inflatable ring 56 may be inflated through conventional inflation techniques such as, for example, the addition to the inflatable ring 56 of air via a syringe. Inflatable
15 ring 56 maybe deflated through the reverse process. One advantage of the inflatable ring 56 over the inflatable cuff 54 is that the external ear canal is not occluded when the electrode 10 is in place. The lack of occlusion of the external ear canal may be advantageous in those
20 situations where the electrode 10 has been utilized for recording purposes. Thus, the tympanic membrane 48 could still receive conventional auditory waveforms through the external ear canal without the external ear canal being obstructed.

25 The electrode 10 illustrated in Figure 7 contains the silicone elastomeric tubing 12 and compressible material 18 and conductive gel 20 at distal end 16 as well as electrical conductor 22. The electrode 10 of Figure 7 for mechanical fixation carries a cone-shaped
30 collar 58 affixed to silicone elastomeric tubing 12. The collar 58 may be constructed from a transparent silicone elastomeric material which would afford visability through the external ear canal by the technician while the electrode 10 is being inserted. The narrow end of
35 the cone of the collar 58 is toward the distal end 16

of the electrode 10. Thus, the electrode 10 would be easily inserted into the ear canal and the collar 58 would take the form of the external ear canal and mechanically fix and hold the electrode 10 in place.

5 The electrode 10 illustrated in Figure 8 is similar. Again, silicone elastomeric tubing 12 carries electrical conductor 22 to the distal end 16 where the compressible material and conductive gel are located. For mechanical fixation, the electrode 10 carries
10 stabilizing fins 60 affixed to the silicone elastomeric tubing 12. These fins 60 may be constructed of the same silicone elastomeric material as silicone elastomer tubing 12. The fins are affixed to the silicone elastomer tubing 12 and radiate outward and back away from distal
15 end 16 of electrode 10. Thus, the fins 60 perform a springlike effect when the electrode 10 is inserted into the external ear canal and serve to mechanically hold it in place. Since the fins 60 do not completely transversely surround silicone elastomer tubing 12,
20 the external ear canal is not occluded and the health care technician may visually observe the tympanic membrane while the electrode 10 is being inserted and the external ear canal has left unoccluded following insertion.

 The electrode 10 illustrated in Figure 9 shows
25 the silicone elastomer tubing 12 being utilized in conjunction with a conventional speculum 62. Again, electrical conductor 22 communicates with silicone elastomer tubing 12 to the compressible material and conductive gel 20 at distal end 16 of the electrode 10. Speculum
30 62 is of conventional speculum design. The speculum is slideably attached to the silicone elastomer tubing 12 at its narrowest opening. The advantages in the use of speculum 62 with the electrode 10 are that conventional ear health care specialists are very familiar with the
35 speculum and could use it as a guide in placing the

electrode proximate the tympanic membrane or the
tympano-meatal annulus. Again, the interior of the speculum
62 may be utilized by the health care specialist to
visualize the external ear canal and tympanic membrane
5 during the insertion of the electrode 10 into the external
ear canal 46. An optional feature of the electrode 10
illustrated in Figure 9 is the use of auxiliary tube
64. Auxiliary tube 64 is coupled longitudinally to silicone
elastomer tubing 12 may be utilized either in conjunction
10 with speculum 62 or separately from speculum 62. Through
the use of auxiliary tube 64 once the electrode 10
is placed in the external ear canal proximate the tympanic
membrane or tympano-meatal annulus an anesthetic may
be delivered through the auxiliary tube 64 to the
15 stimulation site of the electrode 10, thus, creating
a locally anesthetized area thereby permitting the
attainment of higher current densities at that location.
It is to be recognized, of course, that auxiliary tube
64 is shown in Figure 9 for illustrative purposes and
20 auxiliary tubes 64 could take many other forms and shapes
within the scope of the present invention. Auxiliary
tube 64 could alternatively be located within the interior
of silicone elastomeric tubing 12 or could take such
other forms as would facilitate the delivery of an
25 anesthetic to the distal end 16 of the electrode once
the electrode 10 has been inserted into the external
ear canal. In one embodiment speculum 62 has a conductive
band 68 on the exterior of the speculum 62 to serve
as a return/reference electrode.

30 Figure 10 illustrates an alternative embodiment
of the electrode 10 of the present invention. Again,
silicone elastomer tubing 12 comprises the elongated
flexible body of the electrode 10. Again, electrical
conductor 22 communicates with silicone elastomer tubing
35 12 to a compressible material 18 and a conductive gel

20 at the distal end 16 of the electrode 10. As an additional cushioning means in order to increase the amount of comfort given by the electrode 10 of the present invention a coiled spring 66 is provided between the
5 compressible material 18 and the silicone elastomer tubing 12 at the distal end 16 of the electrode 10. As the compressible material compresses the tympanic membrane 48 coiled spring 66 would contract giving additional flexibility to the electrode 10 and in addition
10 to that flexibility achieved by the compressible material 18 and silicone elastomer tubing 12.

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CLAIMS:

1. An electrode adapted to be utilized within the external ear canal for applying/recording electrical signals to/from the neural/neuromuscular system of a person having an external ear canal and adjacent tympanic membrane, characterized by having
- 5 an elongate flexible body having a proximate end and a distal end;
a compressible material mounted at said distal end of said body;
10 an electrically conductive gel carried by said compressible material; and
an electrical conductor communicating with said body, said electrical conductor being electrically coupled to said electrically conductive gel and adapted to be coupled to a stimulator/recorder at said proximate end;
- 15 whereby said electrode may be placed in the external ear canal with said distal end being proximate the tympanic membrane or tympano-meatal annulus so that neural/neuromuscular system may be electrically stimulated/recorded.
2. An electrode as in claim 1 wherein said compressible material is absorbent and said electrically conductive gel is absorbed into said compressible material.
- 25 3. An electrode as in claim 2 wherein said compressible material is also resilient.
4. An electrode as in claim 1 wherein said elongated flexible body is stiff enough to be inserted into the external ear canal but flexible enough to bend if said electrode is inserted against the tympanic membrane without rupturing the tympanic membrane.
- 30 5. An electrode as in claim 1 which further comprises an anesthetic being carried by said compressible material.

6. An electrode as in claim 1 which further comprises fixation means for physically securing said electrode with respect to the external ear canal, said fixation means being coupled to said body.

5 7. An electrode as in claim 1 wherein said compressible material comprises a sponge.

8. An electrode as in claim 1 wherein said body comprises silicone elastomeric tubing.

10 9. An electrode as in claim 1 wherein said compressible material is connected to said distal end of said silicone elastomeric tubing by a coiled spring.

10. An electrode as in claim 9 wherein said coiled spring comprises said electrical conductor.

15 11. An electrode as in claim 1 wherein said elongated flexible body is electrically conductive and serves as said electrical conductor.

12. An electrode as in claim 1 wherein said electrical conductor has a resistance of not more than about ten kilohms.

20 13. An electrode as in claim 1 wherein said body has a first portion which is more flexible than a second portion of said body, said second portion of said body being closer to said distal end than said first portion.

25 14. A method of stimulating the neural/neuromuscular system of a person having a body and an external ear canal and adjacent tympanic membrane and tympano-meatal annulus, characterized by the steps of:

30 inserting a first electrode into said external ear canal of said person, said first electrode having an elongated flexible body having a proximate end and a distal end, having a compressible material mounted at said distal end of said body, having an electrically
35 conductive gel carried by said compressible material, having an electrical conductor communicating with said elongated flexible body being electrically coupled to said electrically conductive gel, said first electrode

being positioned with said electrically conductive gel proximate said tympanic membrane or tympano-meatal annulus of said person;

5 applying a second electrode to said body of said person; and

 applying an electrical stimulus signal to the electrode pair comprising said first electrode and said second electrode.

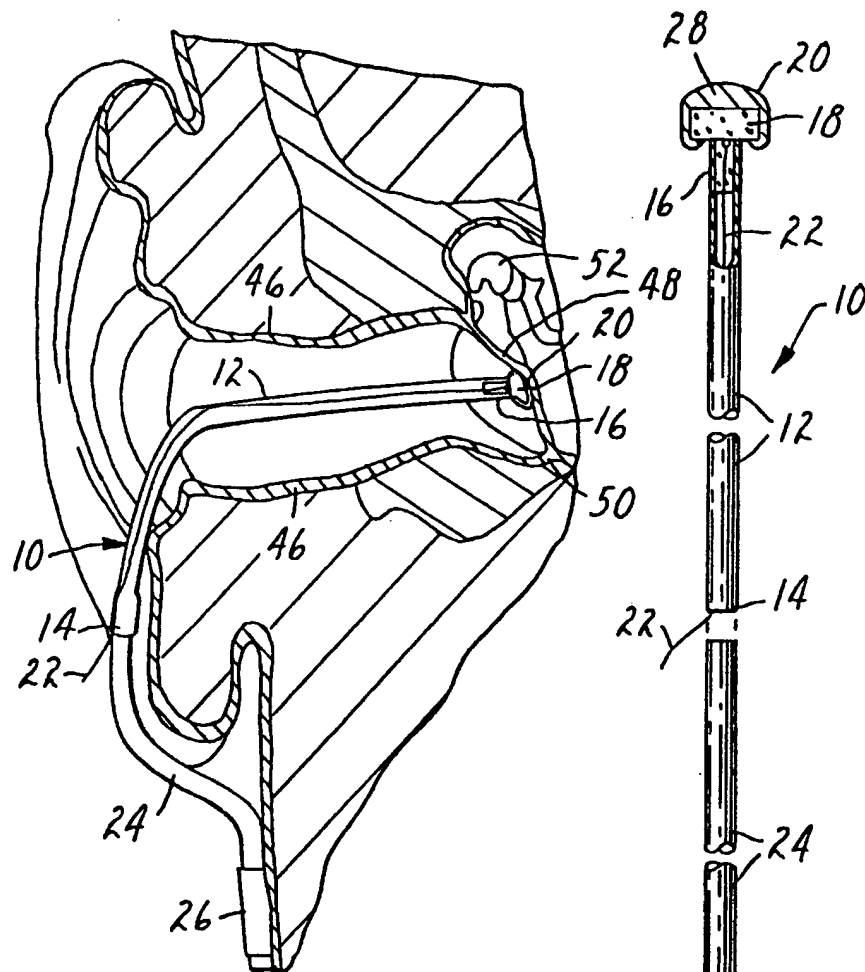
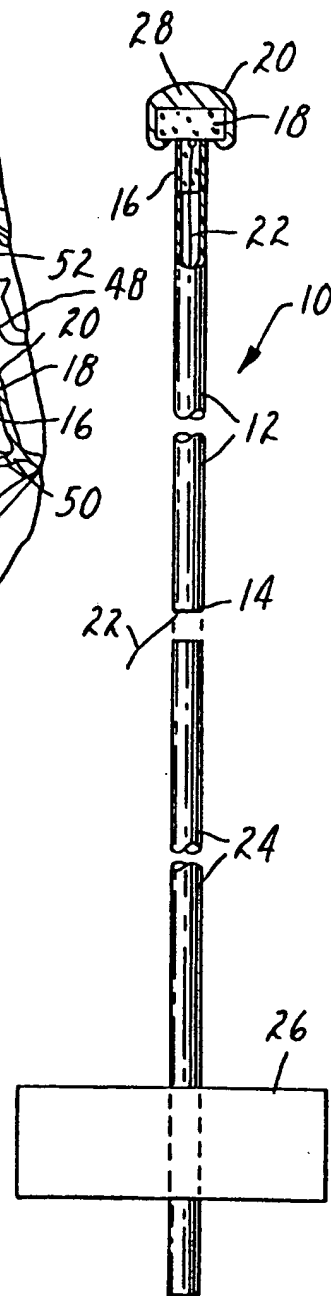
15 15. A method of stimulating the neural/neuromuscular system of a person as in claim 14 which further comprises the step of applying an anesthetic to the area of said tympanic membrane/tympano-meatal annulus of said person.

15 16. A method of recording electrical signals from the neural/neuromuscular system of a person having a body and an external ear canal and adjacent tympanic membrane and tympano-meatal annulus characterized by the steps of:

20 inserting a first electrode into said external ear canal of said person, said first electrode having an elongated flexible body having a proximate end and a distal end, having a compressible material amounted at said distal end of said body, having an electrically conductive gel carried by said compressible material,
25 having an electrical conductor communicating with said elongated flexible body being electrically coupled to said electrically conductive gel, said first electrode being positioned with said electrically conductive gel proximate said tympanic membrane or tympano-meatal annulus
30 of said person;

 applying a second electrode to said body of said person; and

35 recording the electrical signal obtained from the electrode pair comprising said first electrode and said second electrode.

**FIG. 4****FIG. 1**

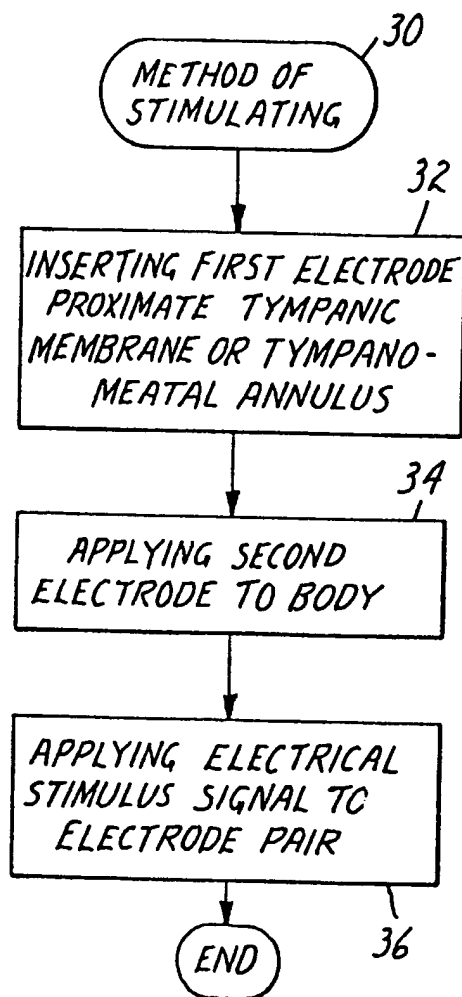


FIG. 2

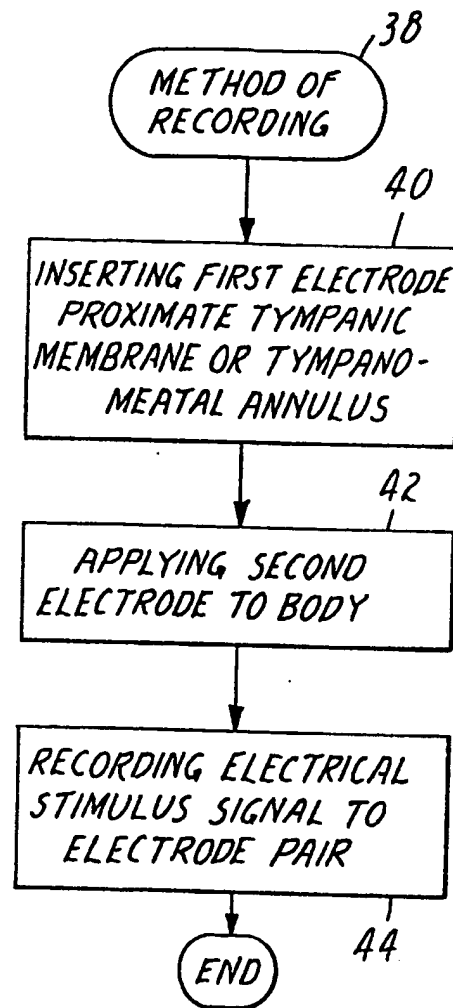


FIG. 3

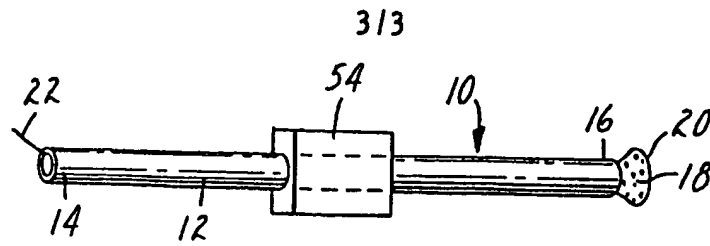


FIG. 5

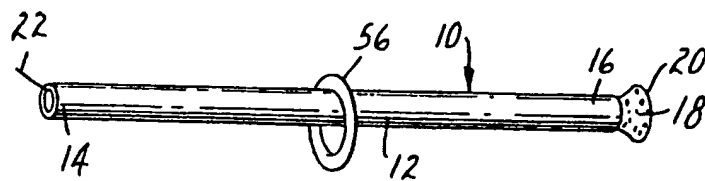


FIG. 6

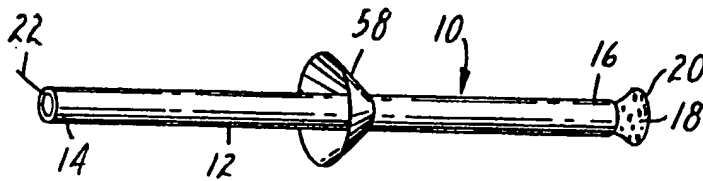


FIG. 7

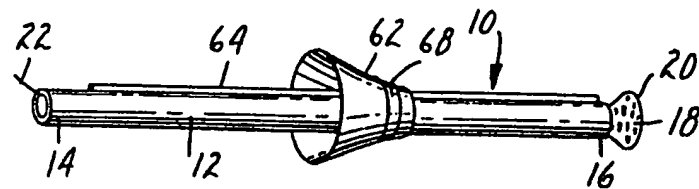


FIG. 9

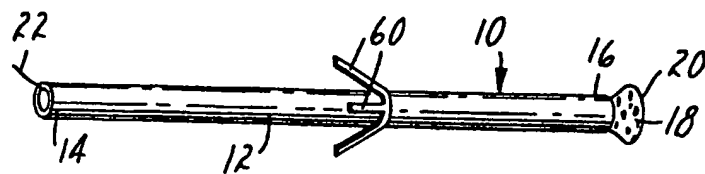


FIG. 8

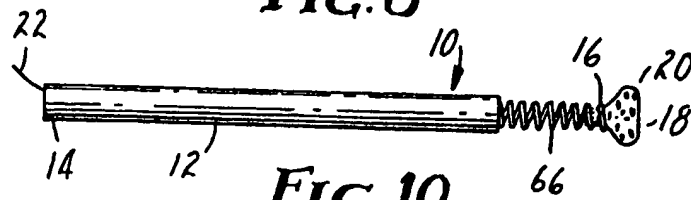


FIG. 10



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DOCUMENTS CONSIDERED TO BE RELEVANT			
Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (Int. Cl.)
Y	EP - A - 0 084 972 (AXONICS, INC.) * claims 1, 9; page 10, lines 6-15; figure 6 *	1	A 61 F 11/04 A 61 B 5/12 A 61 N 1/05
A	--	2,3	
Y	DE - A - 3 006 472 (ELECTROCHEMICAL TECHNOLOGY CORP.) * claim 1; figure 1 *	1	
Y	DD - A - 105 720 (GRITTNER) * claim 1; figure 1 *	1	
A	EP - A - 0 104 924 (MINNESOTA MINING AND MANUFACTURING COMP.) * claim 1 *	1-3	
			TECHNICAL FIELDS SEARCHED (Int. Cl.)
			A 61 B 5/00 A 61 F 2/00 A 61 F 11/00 A 61 N 1/00 H 04 R 25/00
INCOMPLETE SEARCH The Search Division considers that the present European patent application does not comply with the provisions of the European Patent Convention to such an extent that it is not possible to carry out a meaningful search into the state of the art on the basis of the information provided. Claims searched completely 1-13 Claims searched incompletely 14-16 Claims not searched Reason for the limitation of the search: Method for treatment of the human or animal body by therapy and diagnostic methods practised on the human or animal body (Article 52 (4)).			
Place of search Berlin		Date of completion of the search 4-12-1986	Examiner KANAL
CATEGORY OF CITED DOCUMENTS X particularly relevant if taken alone Y particularly relevant if combined with another document of the same category A technological background O non-written disclosure P intermediate document I theory or principle underlying the invention E earlier patent document, but published on or after the filing date D document cited in the application L document cited for other reasons & member of the same patent family, corresponding document			

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DOCUMENTS CONSIDERED TO BE RELEVANT			CLASSIFICATION OF THE APPLICATION (Int. Cl.)
Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	
A	<p>EP - A - 0 057 450 (MEDTRONIC, INC.)</p> <p>* claim 1 *</p> <p>--</p>	1	
A	<p>US - A - 3 531 992 (MOORE)</p> <p>* figures 1-3; claim 1 *</p> <p>----</p>	1	
			TECHNICAL FIELDS SEARCHED (Int. Cl.)

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